

The role of NPL in supporting the traceability for dosimetry in emerging techniques - FLASH Radiotherapy

[Anna Subiel](#)

Medical Radiation Science, National Physical Laboratory,
Hampton Road, Teddington, Middlesex, TW11 0LW, UK

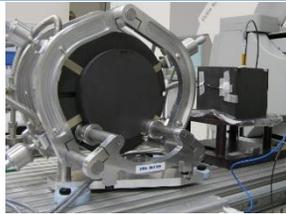
Metrology covers three main tasks:

1. The definition of internationally accepted units of measurement



2. The realization of units of measurement by scientific methods

primary standard



secondary standard



working standard



3. The establishment of **traceability** chains



property of a measurement result whereby the result can be related to a reference through a documented unbroken chain of calibrations, each contributing to the measurement uncertainty

$$M = m \pm U \quad (k = 1)$$

↑ measurand

↑ Measurement uncertainty

↑ coverage factor

Traceability chain in Radiotherapy

- MV photon dosimetry under reference conditions



σ : 0.50 % (k=1)

0.7 % (k=1)

1.5 % (k=1)

Traceability chain in Radiotherapy

- MV photon dosimetry under reference conditions



σ : 0.50 % (k=1)

0.7 % (k=1)

1.5 % (k=1)

← TRACEABILITY

Why do we need metrology in FLASH RT?

- To compare different measurements carried out in space and time

Timeline of FLASH RT...



Timeline of FLASH RT...

Published: 19 August 1967

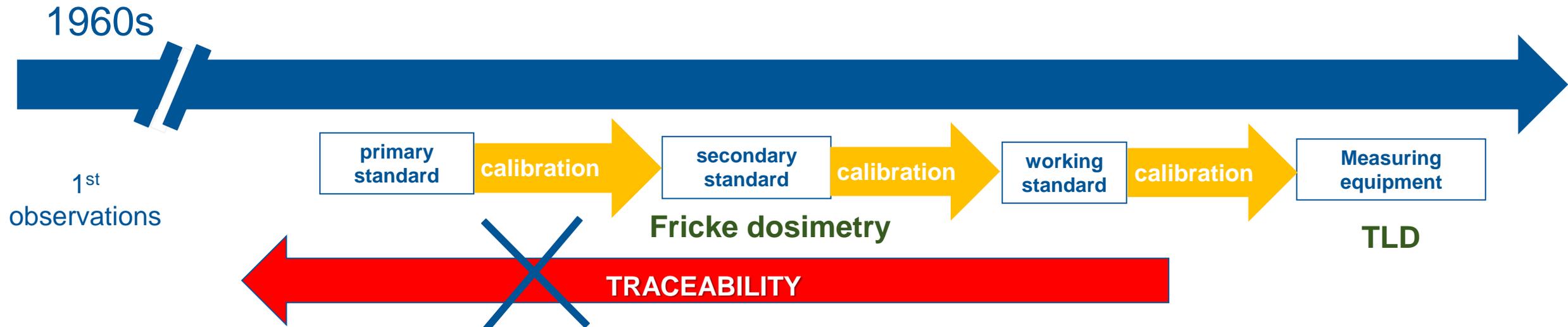
Effect of High Dose Rates on Survival of Mammalian Cells

C. D. TOWN

Nature 215, 847–848 (1967) | [Cite this article](#)

The dose delivered was measured by using lithium fluoride thermoluminescence dosimetry; this was checked by ferrous sulphate and red 'Perspex' dosimetry². The error in the dose delivered, chiefly caused by the spatial distribution of the beam, was 2 per cent at 200 rads, rising to 10 per cent at 5,000 rads.

Is the dose measurement traceable?



Fricke dosimetry in UHDR pulsed e-beams



$$D_W = \frac{\Delta A \cdot f_{F/W}}{\rho \cdot l \cdot \varepsilon(\lambda) \cdot G}$$

Change in absorbance
 $A_{\text{irradiated}} - A_{\text{unirradiated}}$

Density of Fricke solution in kg/l

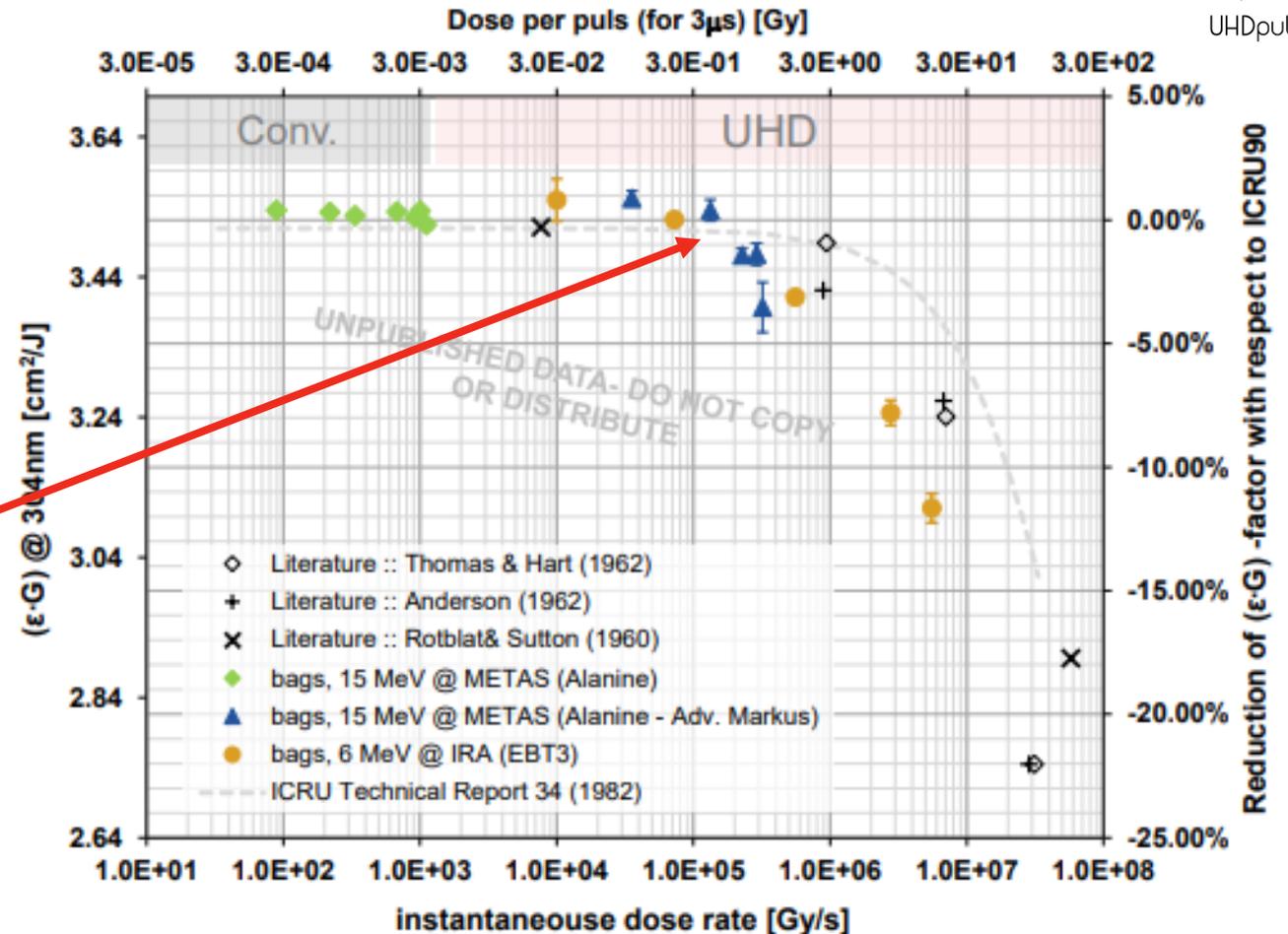
Path length through cuvette in cm

Molar extinction coefficient in l/cm/mol

Chemical yield in mol/J

- At $\sim > 1 \text{ Gy/pulse}$ (of 3 μs) radical-radical reactions start to reduce the value of radiation yield G.

Fricke dosimetry not a primary standard for UHDR e-beam



Courtesy of F. Frei and P. Peier

NOTE: ICRU Rep.34 Fricke solution without NaCl

Timeline of FLASH RT...

Hypoxia in mouse intestine induced by electron irradiation at high dose-rates

SHIRLEY HORNSEY

M. R. C. Experimental Radiopathology Unit, Hammersmith Hospital, Ducane Road, London W.12

and D. K. BEWLEY

Medical Research Council Cyclotron Unit, Hammersmith Hospital, Ducane Road, London W.12

(Received 17 February 1971; accepted 4 March 1971)

Effects of dose-rate on the radiation response of rat skin

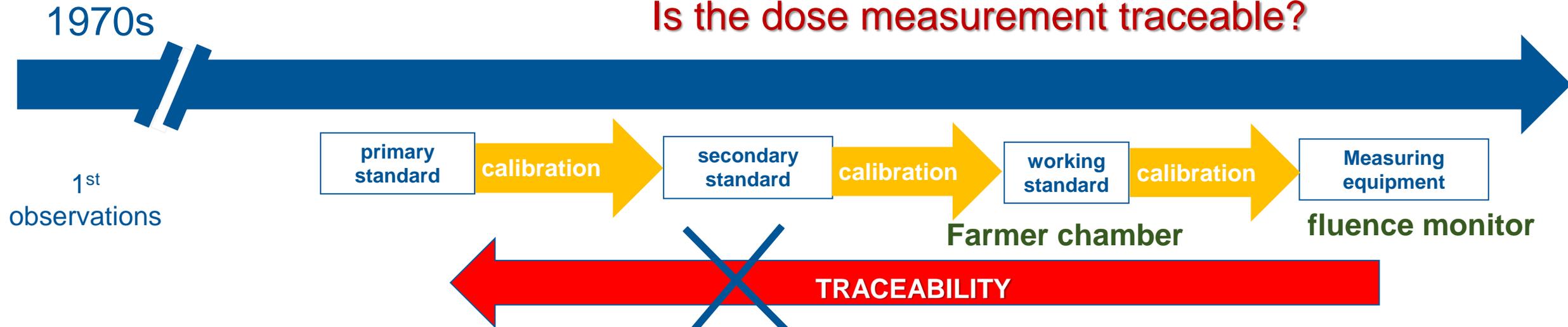
S. B. FIELD and D. K. BEWLEY

Medical Research Council, Cyclotron Unit, Hammersmith Hospital, Ducane Road, London W12 0HS, U.K.

(Received 13 May 1974; accepted 12 June 1974)

In studies of the effects of varying dose-rates, it is essential that the response of the monitor and the dose-distribution within the animal should be independent of dose-rate. The experiments reported here were made using 7 MeV electrons from the M.R.C. linear accelerator. The mice were irradiated two at a time in a Perspex box having compartments of internal dimensions $6 \times 3 \times 3$ cm with the entrance window 0.6 mm thick. The dose and dose-rate were monitored with a pair of collector monitors, as described by Bewley (1971). This type of monitor gives a signal proportioned to fluence (or fluence-rate). Absorbed dose bears a constant relation to fluence at a given electron energy, and the constant of proportionality varies only slowly with electron energy at a few MeV. The monitor was calibrated at 100 rads/min with a Farmer-Baldwin chamber to give the dose at the centre of the compartments of the box. The linear accelerator

Is the dose measurement traceable?



Timeline of FLASH RT...

RADIATION TOXICITY

Ultrahigh dose-rate FLASH irradiation increases the differential response between normal and tumor tissue in mice

Vincent Favaudon,^{1,2*} Laura Caplier,^{3†} Virginie Monceau,^{4,5‡} Frédéric Pouzoulet,^{1,2§} Mano Sayarath,^{1,2¶} Charles Fouillade,^{1,2} Marie-France Poupon,^{1,2||} Isabel Brito,^{6,7} Philippe Hupé,^{6,7,8,9} Jean Bourhis,^{4,5,10} Janet Hall,^{1,2} Jean-Jacques Fontaine,³ Marie-Catherine Vozenin^{4,5,10,11}

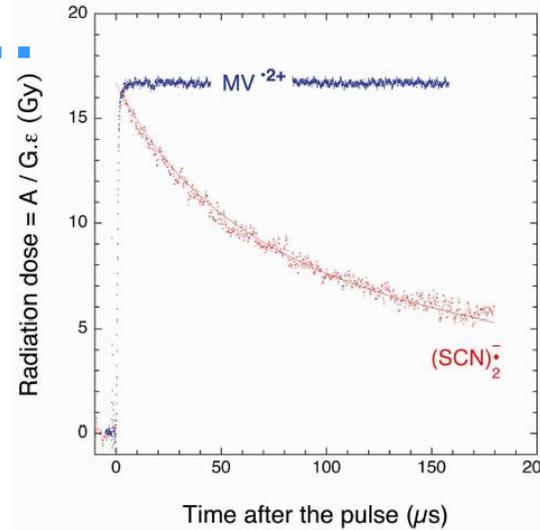


Fig. S4. Time course of the evolution of the methyl viologen MV^{2+} and thiocyanate $(SCN)_2^{-}$ radicals. The evolution of these radicals was measured after a 1.0 μs pulse of 4.5 MeV electrons (16.6 ± 0.1 Gy). The decay of the $(SCN)_2^{-}$ radical occurs by recombination and was fitted (continuous line) to the second-order equation $1/A(t) = 1/A_0 + kt$. Found: $k = 3.74 \times 10^5 \text{ s}^{-1}$.

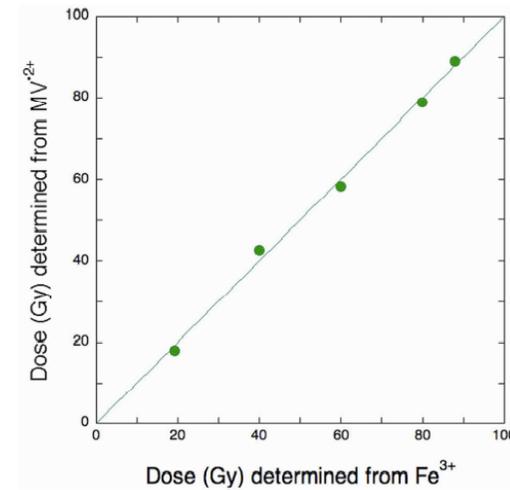


Fig. S5. Correlation between methyl viologen and ferrous sulfate (Fricke) dosimeters. Correlation was established at conventional dose-rate (0.031 Gy/s, ^{137}Cs γ -rays). Fe^{3+} ($\epsilon_{304} = 2,204 \text{ M}^{-1}\text{cm}^{-1}$, $G = 1.61 \mu\text{mol}\cdot\text{J}^{-1}$) and MV^{2+} ($\epsilon_{603} = 13,300 \text{ M}^{-1}\text{cm}^{-1}$, $G = 0.625 \mu\text{mol}\cdot\text{J}^{-1}$) were measured by optical absorption using a Cary-3E spectrophotometer.

1.3 - Dosimetry

Current methods used for the dosimetry of radiation at conventional dose-rate, such as ionisation chambers, do not work at ultra-high dose-rate. For this reason, we used chemical dosimeters long established for pulse radiolysis studies and operating at the submicrosecond time scale. These techniques are described below.

1960s 2014

1st observations

pre-clinical study (mouse model)

calibration

secondary standard

calibration

working standard

calibration

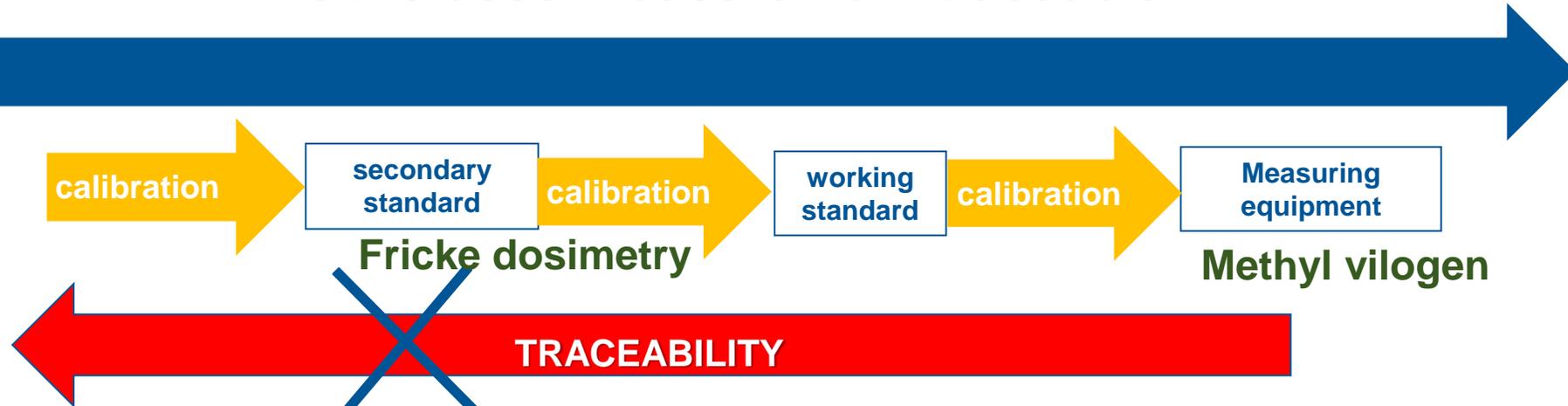
Measuring equipment

Fricke dosimetry

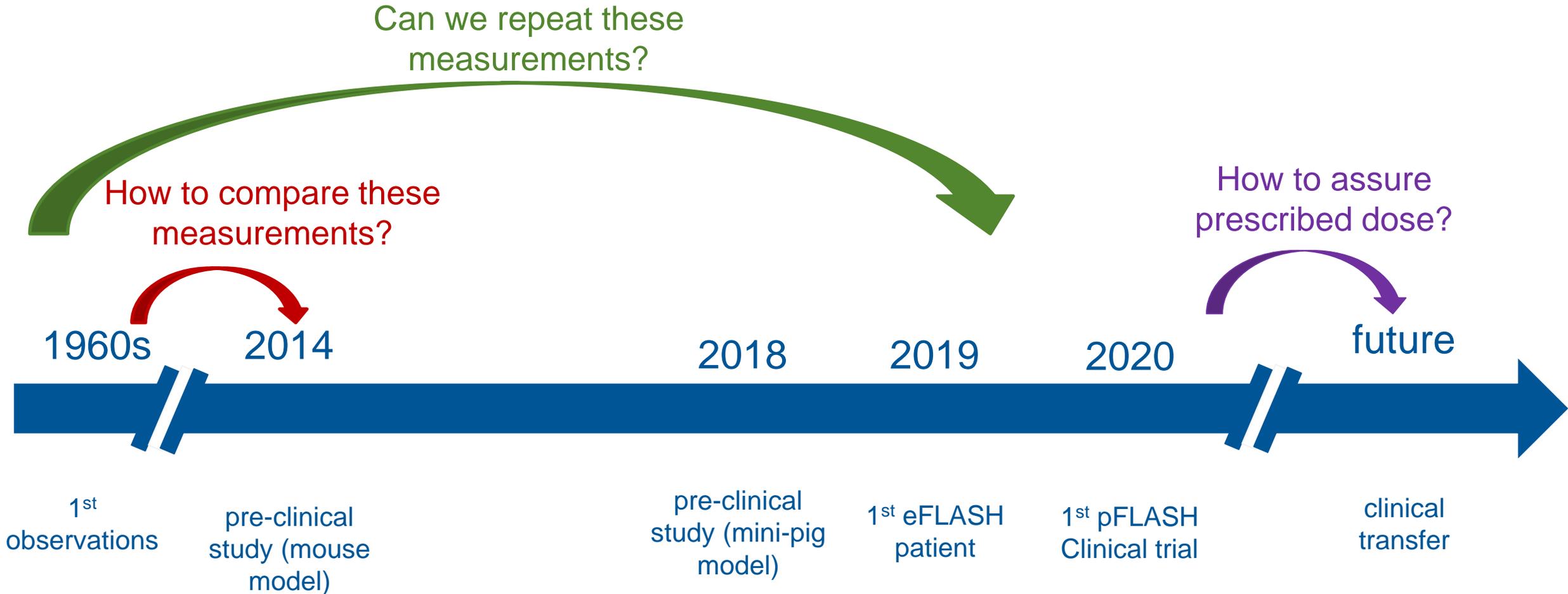
Methyl vilogen

TRACEABILITY

Is the dose measurement traceable?

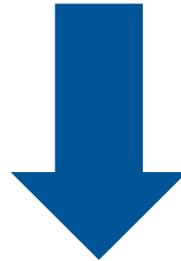


TRACEABILITY IN DOSIMETRY of UHDR beams



Role of National Metrology Institutes

- FLASH community had no support from NMIs with provision of traceability for the UHDR beams
- No standards available
- Developing science and technology that defines the **NEED** for developments in metrology for UHDR exposures



The support needs to come from NMIs
to provide traceable dissemination of D_w to clinics

Requirement for accuracy in dosimetry

- The ICRU Rep.24 (1976) states:

*An uncertainty of **5% (k=1)** is tolerable in the delivery of absorbed dose to the target volume*

This is an **OVERALL UNCERTAINTY**
(incl. dose delivery, dose calculations, patient positioning etc.)

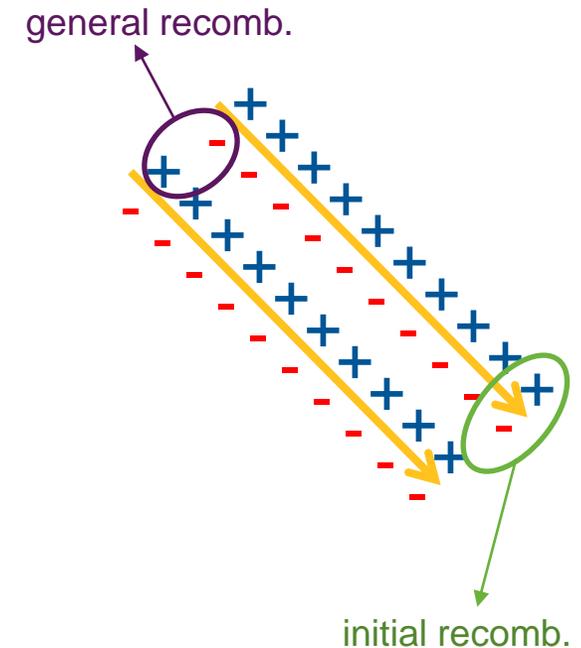
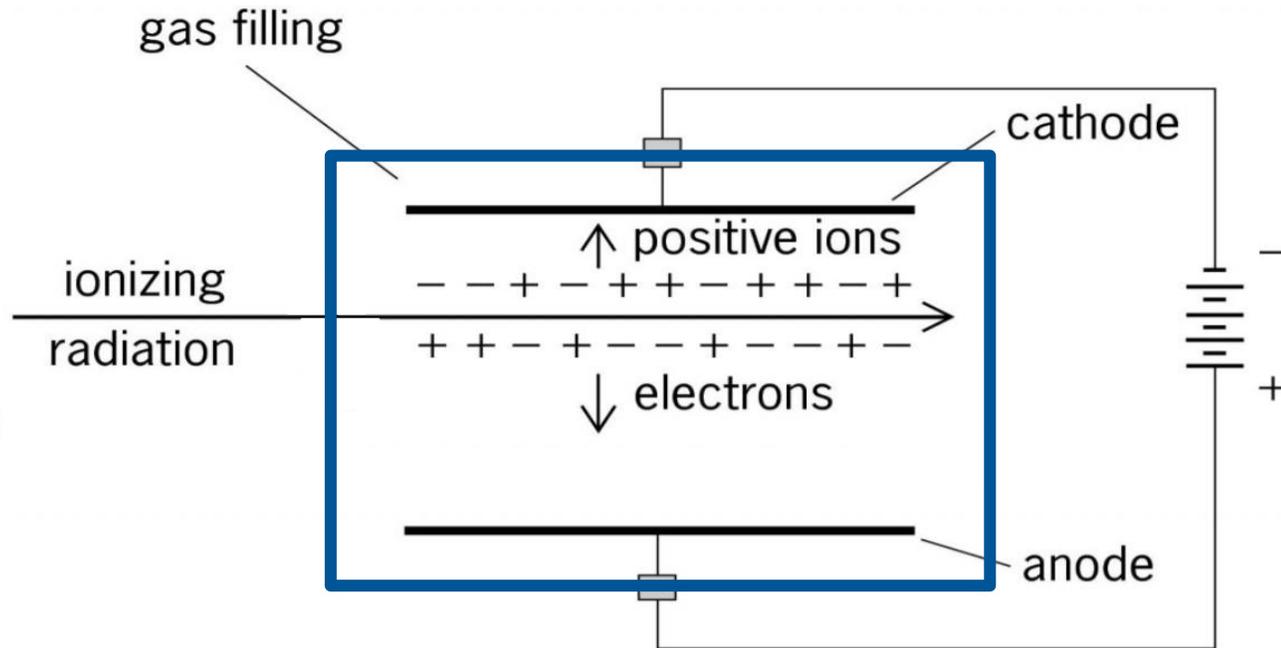


Dose measurement at the reference conditions should to be **less than 1% (k=1)!**

Dosimeters for UHDR

Ionization chambers

Ionization chamber – principle of operation



Initial Recombination

- Recombination along a single charged particle track.
- **Independent of dose and dose-rate.**
- More pronounced in highly ionising particles such as alpha-particles.

General Recombination

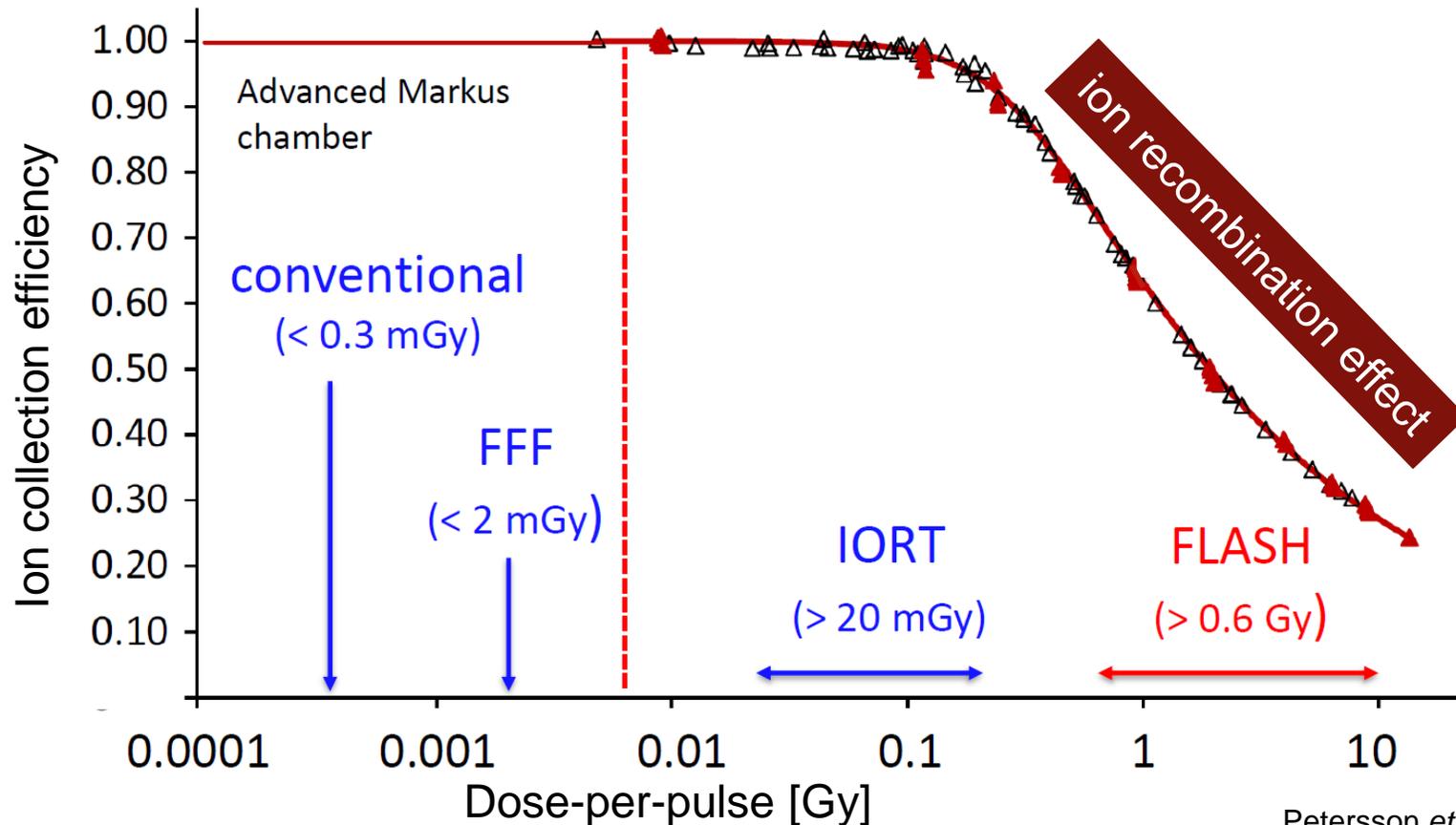
- Recombination between separate charged particle tracks.
- Directly dependent on charge density i.e the number of ions produced per unit volume.
- **Dose-rate dependent.**

General recombination is likely to play a **much larger role** in recombination effect in **UHDR pulsed beams**

IC: Metrological challenges of dosimetry at UHDR

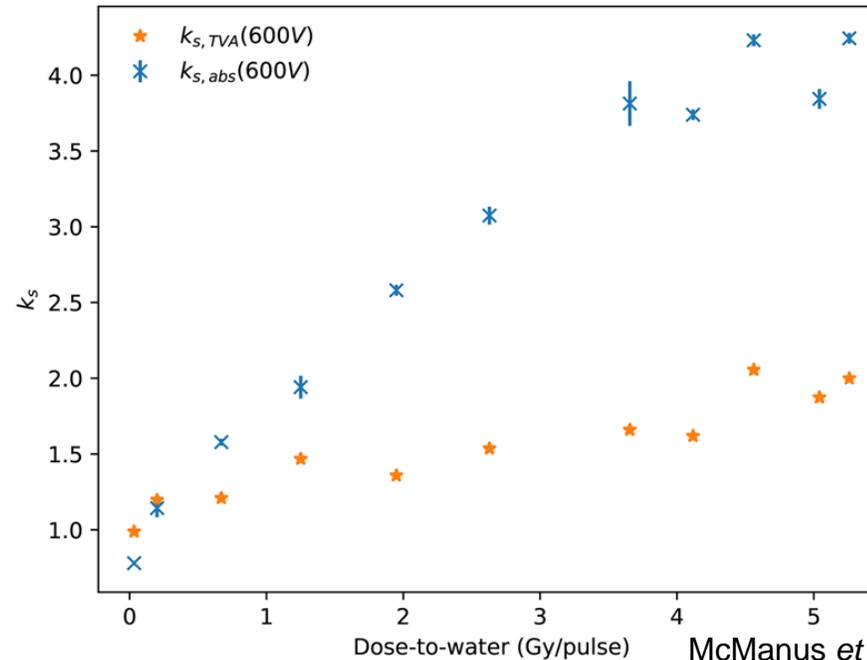
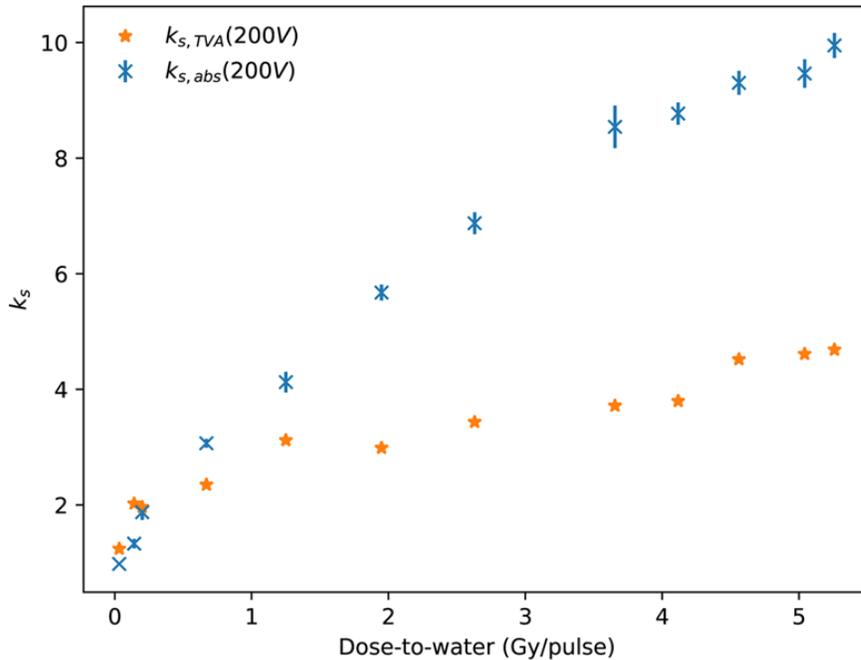
Typical behaviour of an IC at UHDR dose rates for **pulsed electron beams**

6 MeV e-beam



PTW Advanced Markus
(1 mm electrode separation)

IC: Metrological challenges of dosimetry at UHDR

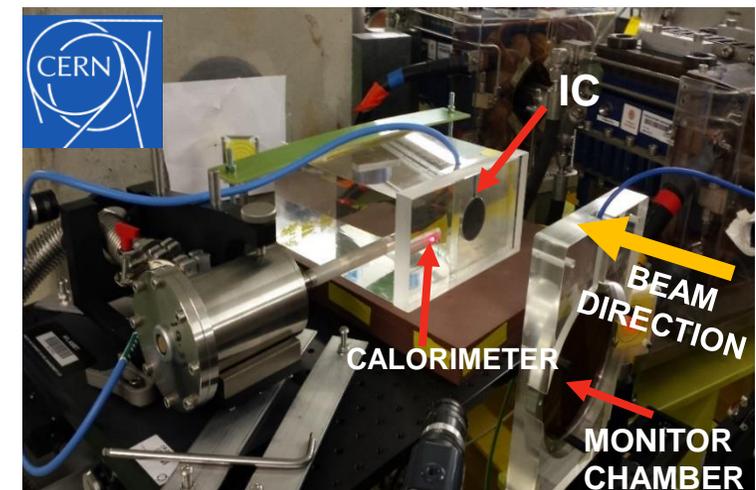


- 200 MeV VHEE beam
- DPP: 0.03 – 5.3 Gy/pulse
- Graphite calorimeter employed as reference detector

$$k_{s,abs} = \frac{D_{w,cal}}{M k_{pol} k_{TP} k_{Q,Q_0} N_{D,w,Q_0}}$$

McManus *et al.*, Sci. Rep. (2020)

- k_s up to 10 ($V = 200\text{ V}$) → **collection eff. 10%**
- k_s up to 4 ($V = 600\text{ V}$) → **collection eff. 25%**
- $k_{s,abs}$ compared with $k_{s,TVA}$ (two-voltage method)
- Available **analytical ion recombination models cannot predict chamber behaviour** for such a high DPP



Ionization chambers – possible solutions

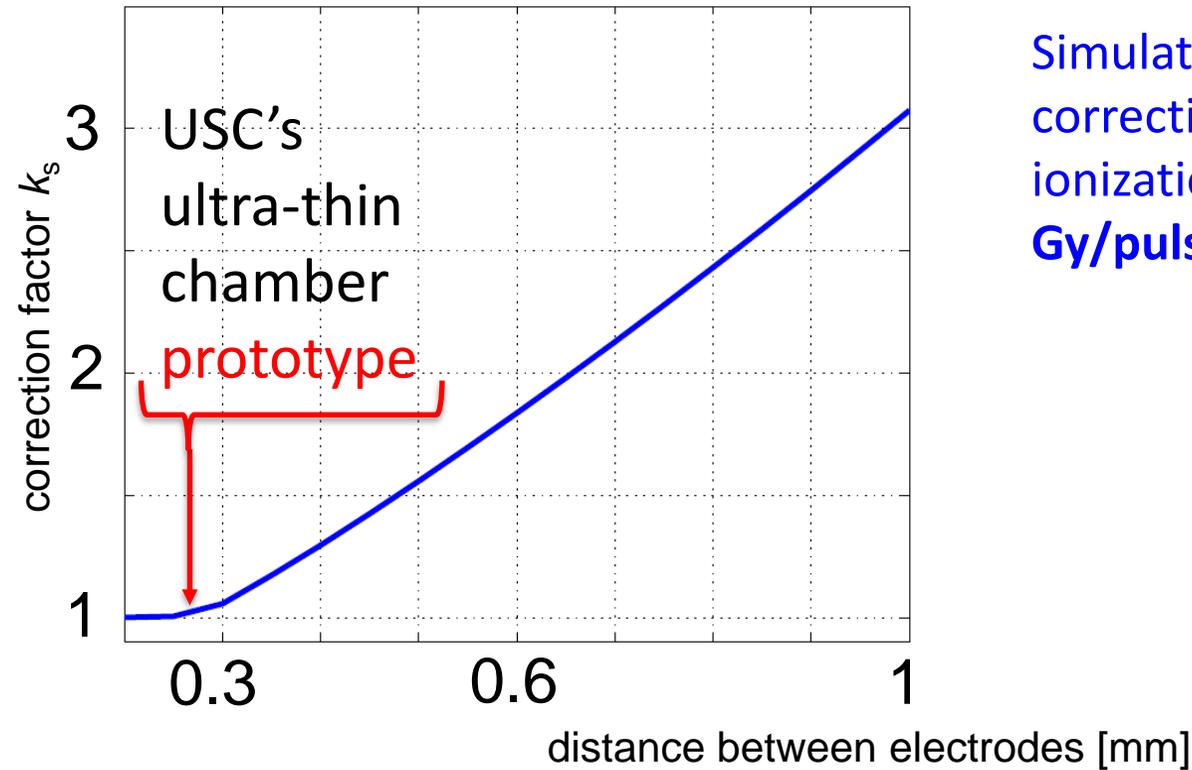
Possible solution for UHDR beams



USC's prototype ionization chambers for ultra-high DPP



Fig. Ionization chamber prototype (0.27 mm)



Simulated ion recombination correction factor k_s for plane parallel ionization chambers at 300 V for 5 Gy/pulse

Courtesy of Faustino Gomez

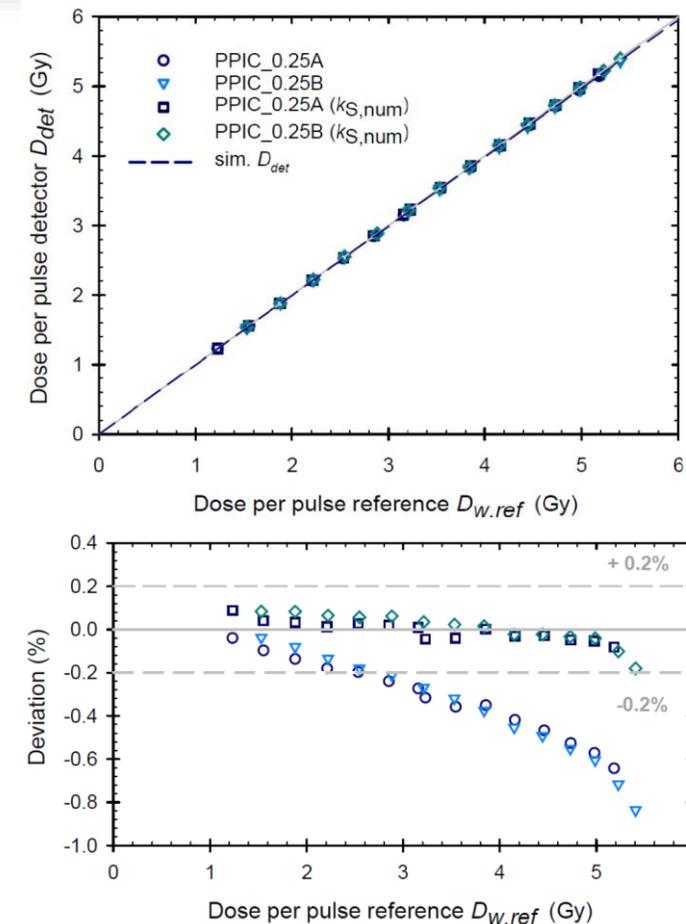
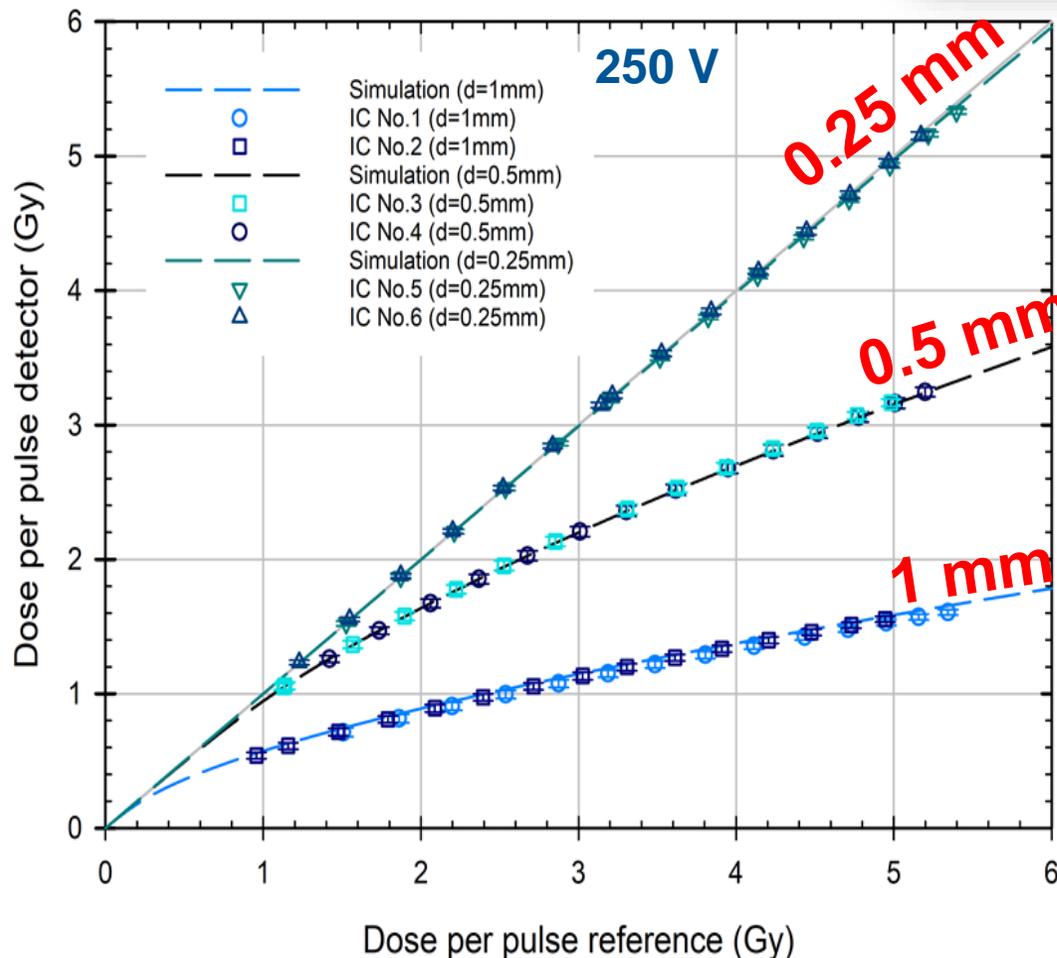
Possible solution for UHDR beams



PTW's prototype ionization chambers for ultra-high DPP



Fig. PTW IC prototype (0.25 mm)



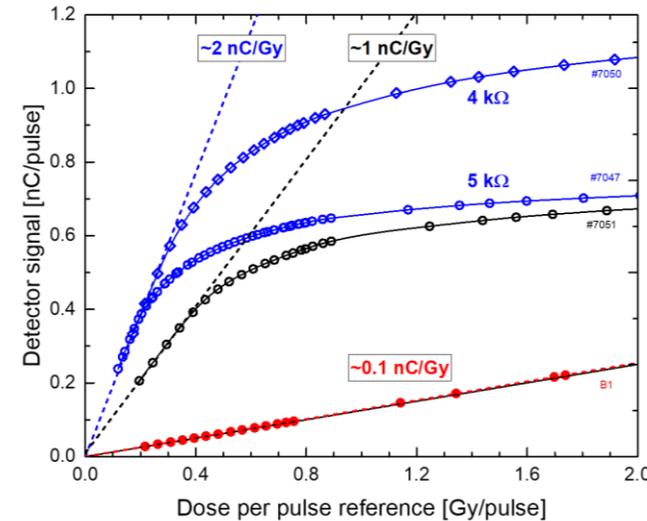
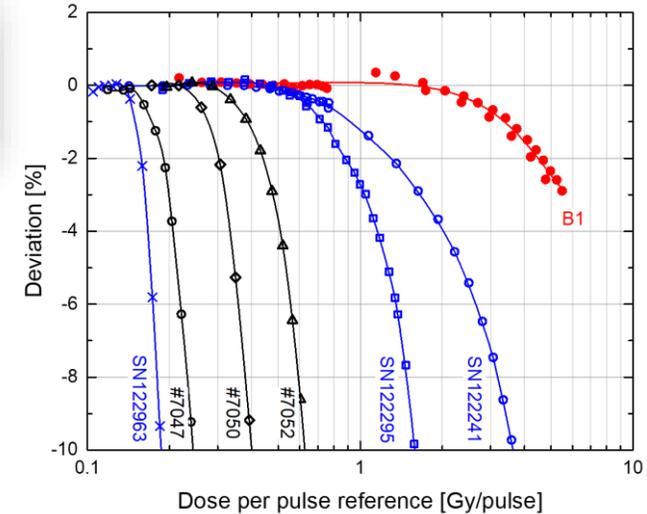
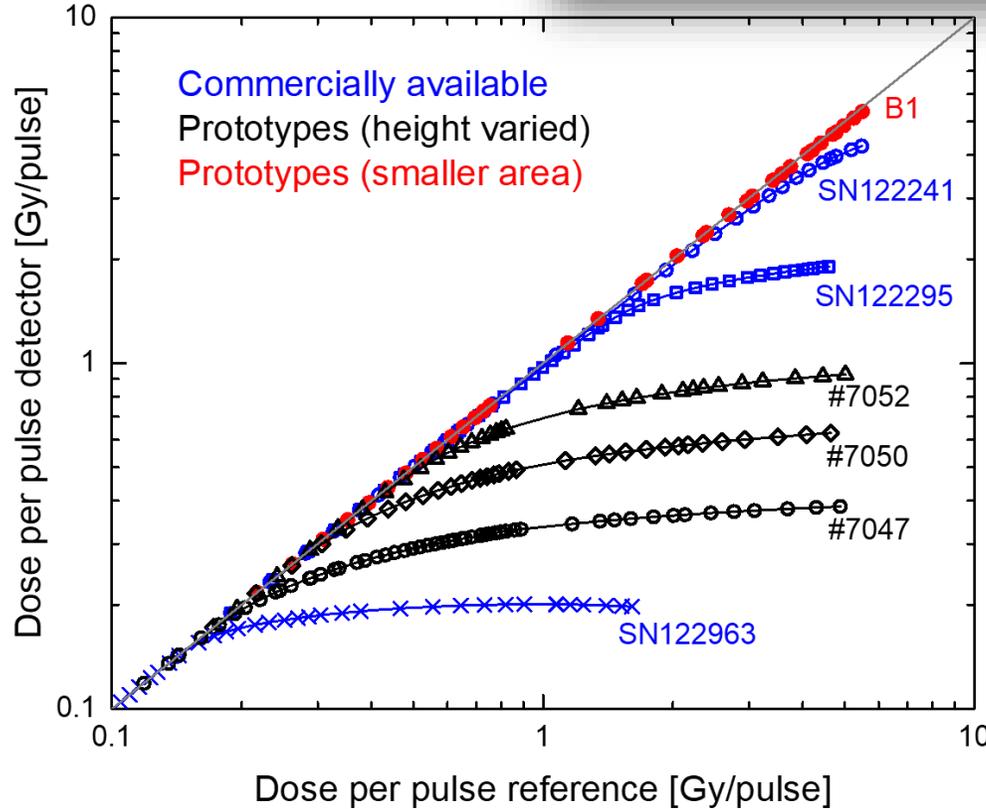
Diamond detectors

Possible solution for UHDR beams

PTW's microDiamond for ultra-high DPP



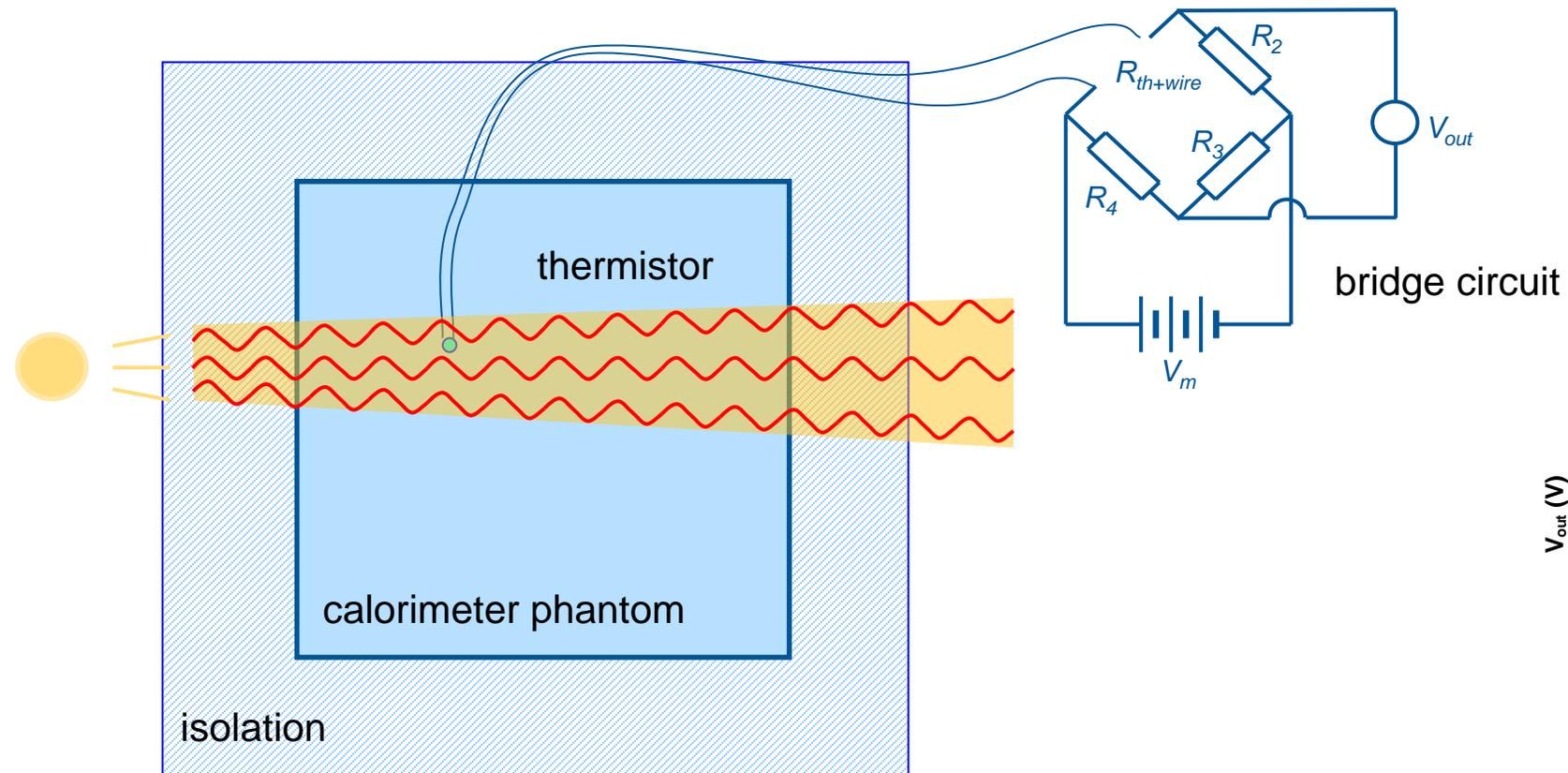
Fig. microDiamond



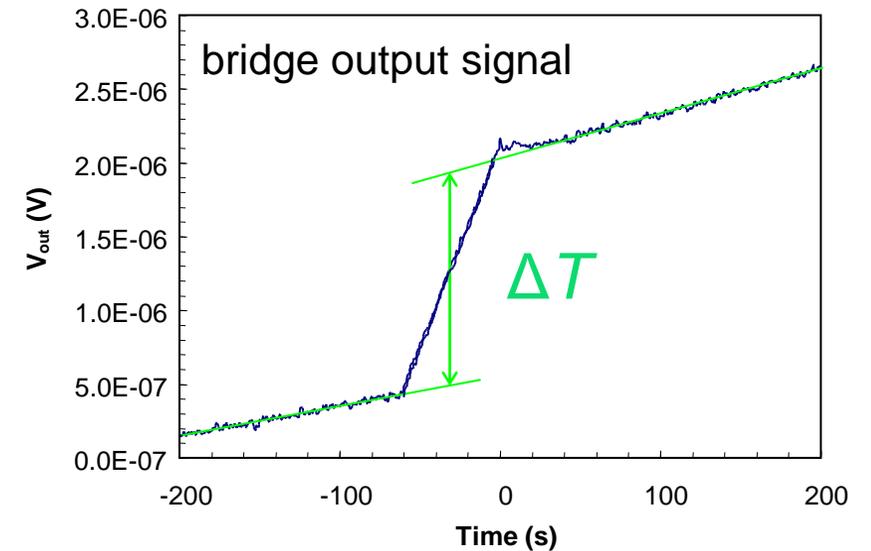
- Commercially available microDiamond detectors show saturation effects at different DPP levels.
- The linear range can be extended to the ultra-high DPP range by reduction of sensitivity and resistance.

Calorimeters

Calorimeters used as prim. standards in high energy beams



$$D=c \cdot \Delta T$$



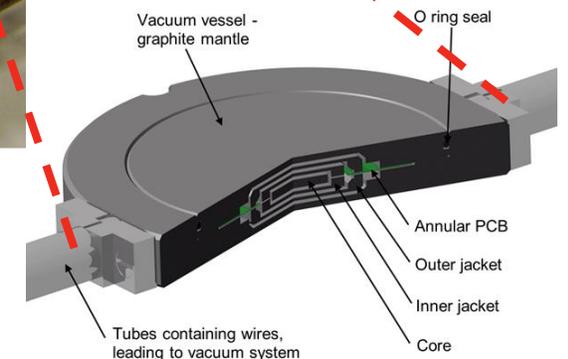
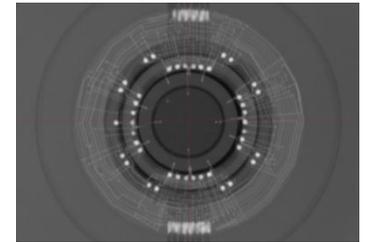
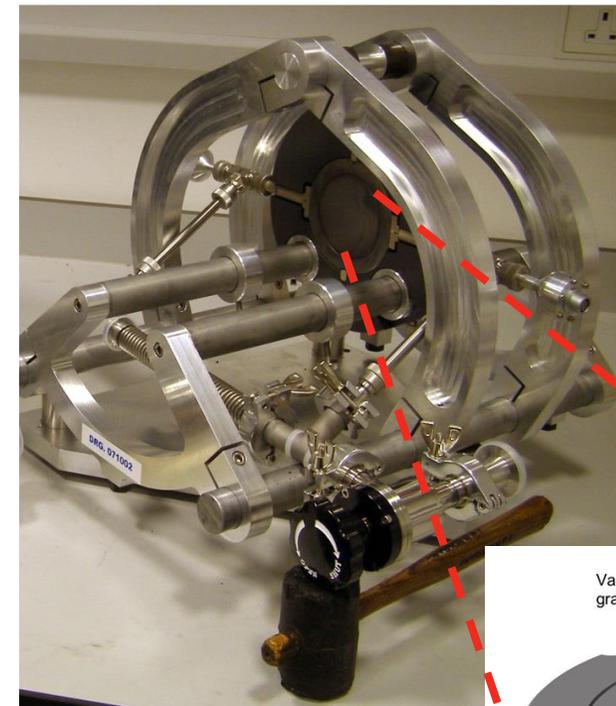
ADVANTAGES

- independent of dose-rate
- linear with dose in UHDR range
- independent of pulse structure
- real-time readout

Calorimetry in UHDR beams

NPL primary standard graphite calorimeter

- the control and analysis software was reconfigured to enable it to be used with UHDR particle beams
- Operated in quasi-adiabatic mode, thermistors detect changes in temperature of the graphite created by energy absorbed from the radiation beam allowing derivation of absorbed dose



NPL's primary standard graphite calorimeter.

Calorimetry in UHDR beams

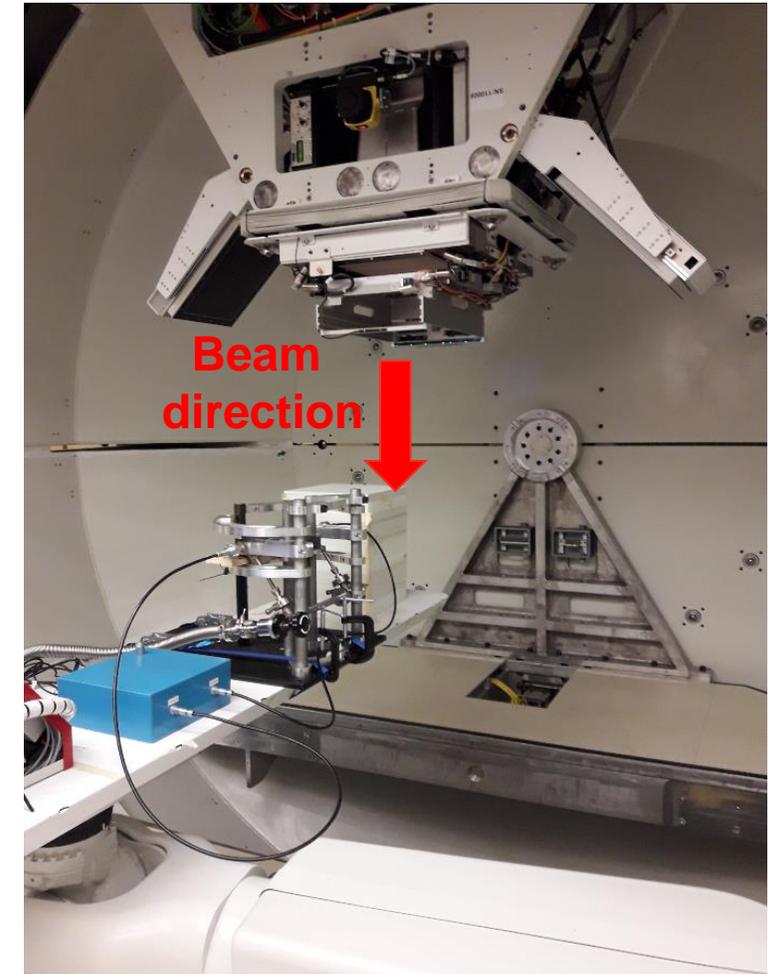
NPL primary standard graphite calorimeter

- 250 MeV (Varian ProBeam® operating in research mode) at ~65 Gy/s
- The core of the calorimeter was positioned at the isocentre with graphite plates placed in front to position the core at a WET of 5 gcm⁻²

Field size, cm	Proton calorimeter				dose to water	
	5 x 6	5 x 8	5 x 10	5 x 12	6 x 5	12 x 5
Mean Dose, Gy	7.654	7.690	7.726	7.736	7.666	7.741
SDOM, %	0.04%	0.04%	0.04%	0.04%	0.04%	0.03%

Parameter	Value	Sources of uncertainties (%)	
		Type A	Type B
c (J·kg ⁻¹ ·K ⁻¹)	651.57+2.74·(T-273.15)	<0.01	0.09
k_{imp}	1.0016	0.20	0.06
k_{gap}	1.0029	0.08	0.26
$s_{w,g}$	1.1210	0.01	0.11
k_{fl}	0.9713	0.07	0.71
$k_{z,cal}$	1.0000	-	0.10
		0.06	0.13
		-	0.25
		0.04	0.15
		0.24	0.84
			0.9

Lourenço *et al.* *Sci.Rep.* under review



Calorimetry in UHDR proton beams



→ First ever calorimetry measurements in UHDR proton beam

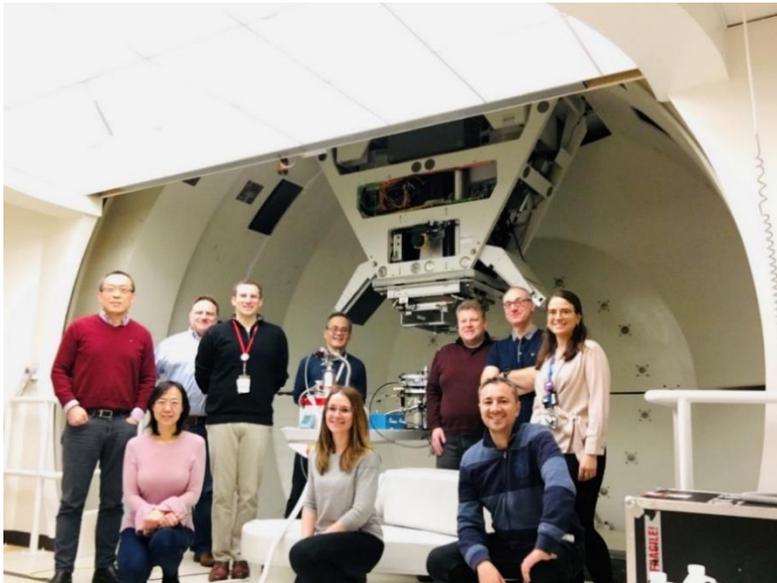
- Established the correction factors required for absolute dosimetry of FLASH proton beam radiotherapy (Lourenço et al., 2022 (under review))
- Measurement uncertainty of 0.9% ($k=1$) – in line with clinical requirement
- **Underpinned the FDA approval and provided the hospital with confidence to commence clinical implementation of this novel technology**



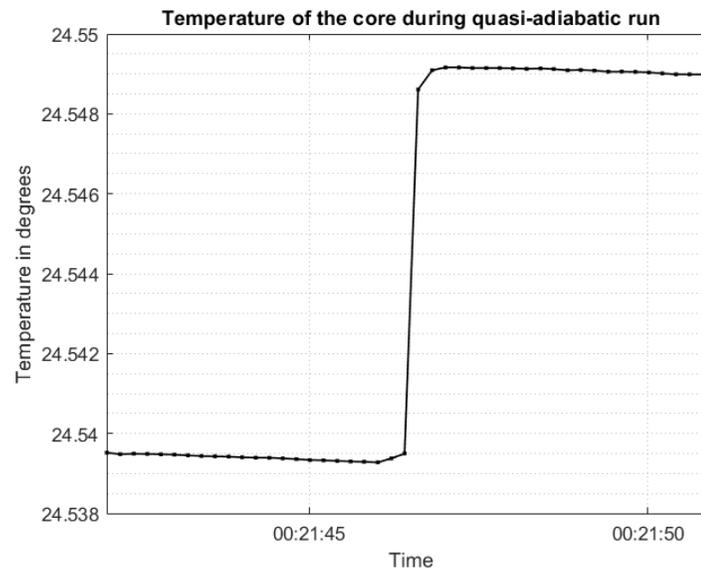
Feasibility Study of FLASH Radiotherapy for the Treatment of Symptomatic Bone Metastases (FAST-01)

ClinicalTrials.gov Identifier: NCT04592887

[Recruitment Status](#) ⓘ : Active, not recruiting
[First Posted](#) ⓘ : October 19, 2020
[Last Update Posted](#) ⓘ : November 1, 2021



NPL and Cincinnati Teams

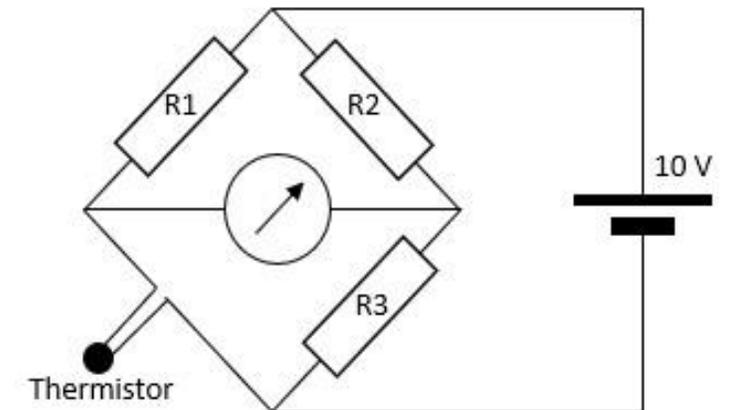
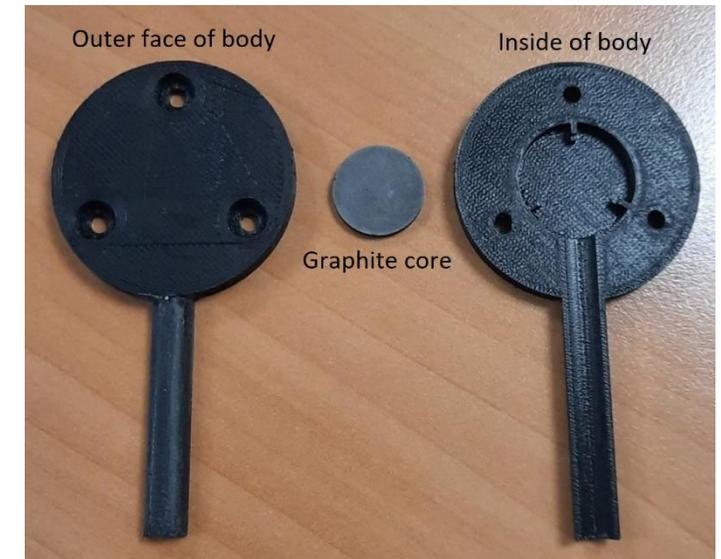


Simple Design Calorimeters as secondary standards for FLASH RT

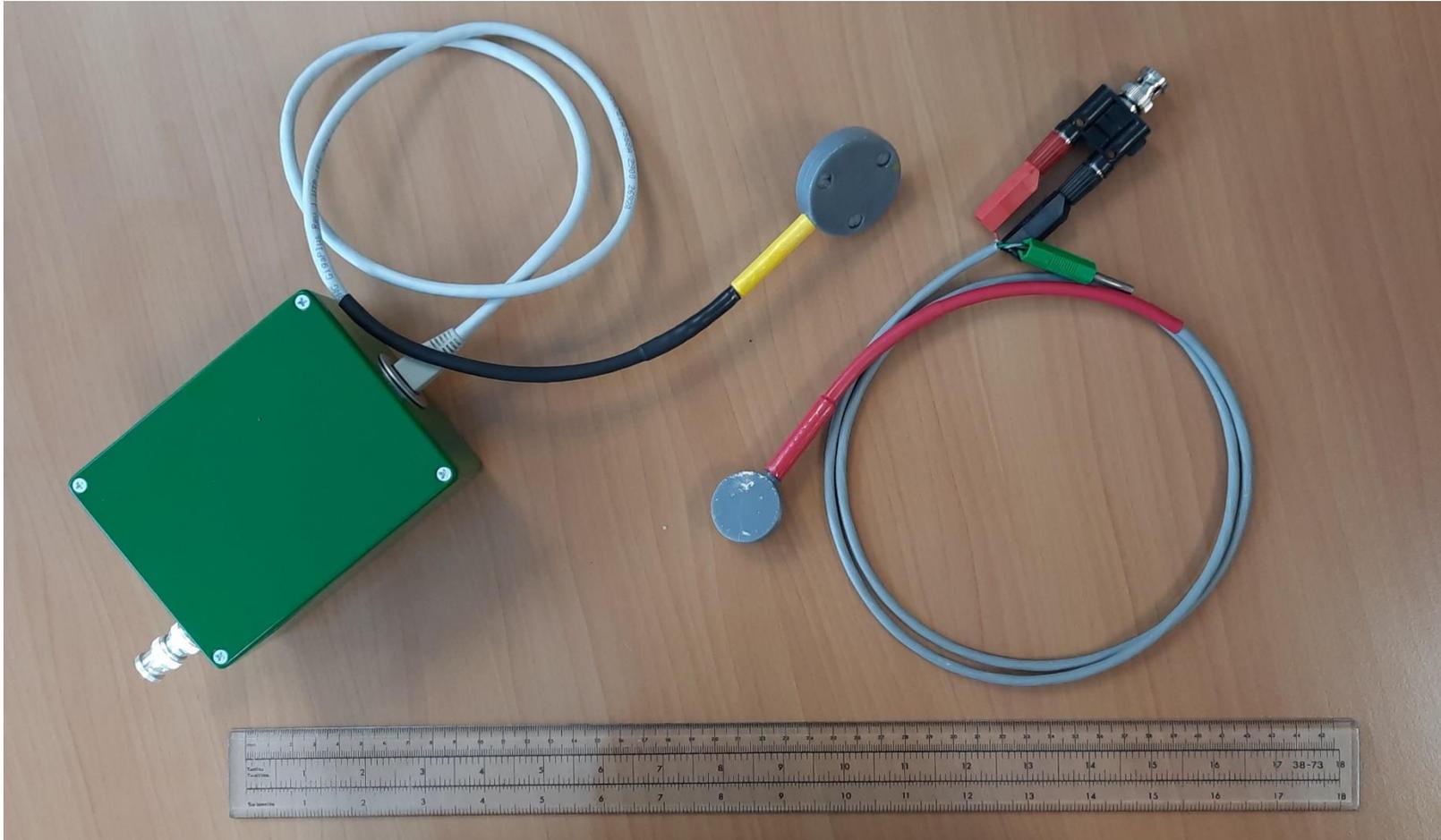
Secondary standard calorimeter: *basic design & measurement system*

- Shaped like a Roos or PPC05 IC
- Solid graphite or aluminium core 16 mm \varnothing , 2 mm thick, supported on 3 plinths, surrounded by air gap
- Single thermistor embedded in core, 10 k Ω at 25 °C
- 3D-printed body, in two halves
- Can be lacquered to be waterproof

- Simple DC Wheatstone bridge
- Sensing thermistor in one arm
- Resistors 10 k Ω \pm 0.01 %, \pm 2 ppm/°C
- 10 V supply voltage



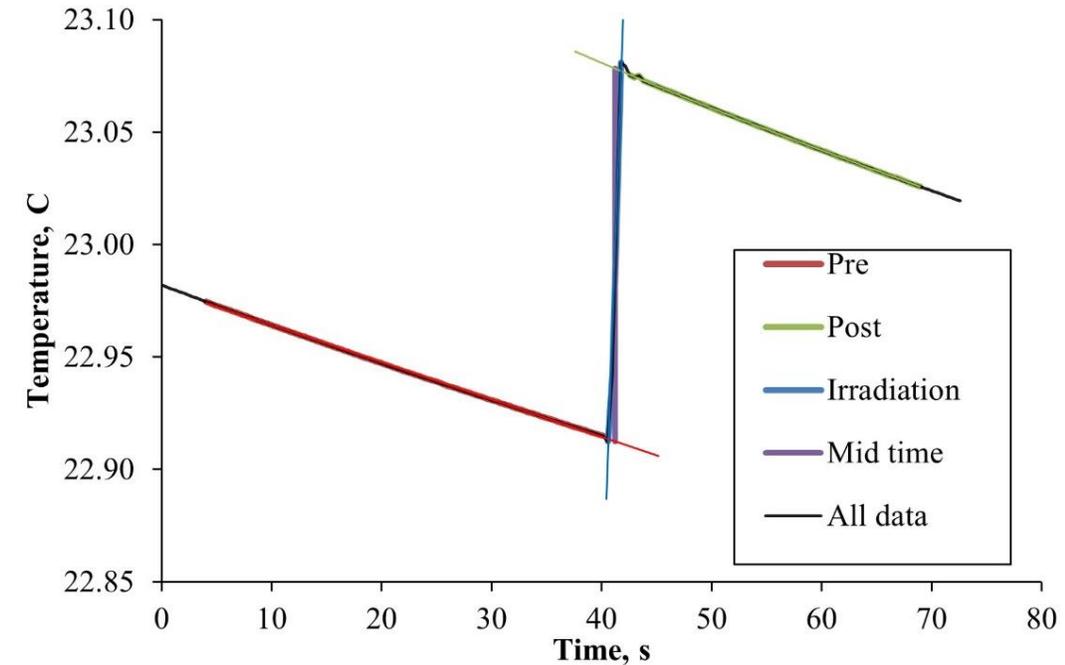
Secondary standard calorimeter: *built examples*



Courtesy of R. Thomas

Secondary standard calorimeter: *UHDR beam response*

- test in research 28 MeV proton beam
- ~100 Gy beam delivery in < 0.5s
- Much higher SNR compared to conv. delivery
- Extrapolation of pre- and post-irradiation drifts over much shorter duration → resulting in lower uncertainty
- Investigations planned in
 - UHDR high energy proton beam
 - UHDR electron beam
 - and more..



How to ensure traceability in FLSH RT?

1. Disseminate the D_w in the UHDR beam with a primary standard
2. Use adequate detectors as a s/s and calibrate them against primary standard under the reference conditions



0.9% (k=1)



1.4 % (k=1)

- The reference conditions need to be specified (TBC) → these will depend on the UHDR radiation device

Summary

- Metrology is essential for **safe** and efficient clinical translation of FLASH RT

This requires:

- Definition of reference beam conditions
 - Dissemination of D_w through a primary standard
 - Establishment for adequate secondary standard devices (thin gap IC, fDiamond or ssCal)
-
- To enable provision of traceability chains in FLASH RT

NOTE: if we move away from IC dosimetry → the dosimetry CoP need to be adjusted for FLASH RT

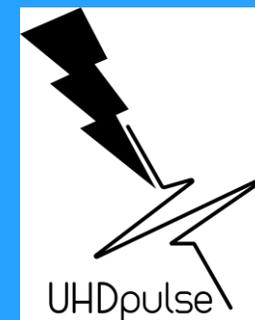
Thank you

anna.subiel@npl.co.uk
russell.thomas@npl.co.uk



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<http://uhdpulse-empir.eu/>